

## Noise enhancement of information transfer in crayfish mechanoreceptors by stochastic resonance

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**IN linear information theory, electrical engineering and neurobiology, random noise has traditionally been viewed as a detriment to information transmission. Stochastic resonance (SR) is a non-linear, statistical dynamics whereby information flow in a multi-state system is enhanced by the presence of optimized, random noise<sup>1-4</sup>. A major consequence of SR for signal reception is that it makes possible substantial improvements in the detection of weak periodic signals. Although SR has recently been demonstrated in several artificial physical systems<sup>5,6</sup>, it may also occur naturally, and an intriguing possibility is that biological systems have evolved the capability to exploit SR by optimizing endogenous sources of noise. Sensory systems are an obvious place to look for SR, as they excel at detecting weak signals in a noisy environment. Here we demonstrate SR using external noise applied to crayfish mechanoreceptor cells. Our results show that individual neurons can provide a physiological substrate for SR in sensory systems.**

The concept of SR originated in efforts to explain the suggested periodicities in recurrences of the Earth's ice ages as the

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result of stochastic and weak periodic forces acting in concert on a bistable, global climate model<sup>7-10</sup>. Subsequent experimental<sup>1</sup> and theoretical<sup>2,3</sup> work demonstrated that the information content of a weak signal can be maximized by noise in certain nonlinear systems. An operational definition of SR is that some measure of the output coherence relative to the output noise passes through a maximum at an optimal value of the input noise.

As a preliminary search for SR in living systems, we have studied the timing of spiking events (action potentials) in single mechanoreceptor cells of the crayfish, *Procambarus clarkii*<sup>11-13</sup>. As spiking can be induced by both noise and a coherent signal, we hypothesized that transmission of a weak mechanical stimulus could be enhanced by an optimal noise intensity. We were guided by an early review on statistical processes in neurons<sup>14</sup> and by previous experiments involving external<sup>15,16</sup> or internal<sup>17-19</sup> noise which, in certain cases, was found to enhance some aspect of the quality of the response<sup>15,20</sup>. In an experimental approach similar to the physical demonstrations of SR, we added an external noise source to a weak periodic signal, defining this combination as the stimulus. We obtained both power spectra (PS) and interspike interval histograms (ISIHs), which assess the coherence of the spiking activity with the signal frequency. An alternative measurement, the peri-stimulus time (cycle) histogram, which is sensitive to coherence with the signal phase is not considered here but is being studied in our laboratory.

Original studies of the ISIH of spontaneous and stimulated discharges in cat auditory fibres and their interpretation in terms of a noisy integrate-and-fire model demonstrated the exponential-like decay of peaks located at integer multiples of the stimulus period<sup>21</sup>. Although both single<sup>22-24</sup> and populations<sup>20</sup> of integrate-and-fire models with noise have suggested<sup>25</sup> that neurons can exhibit a noise-enhanced response, these studies did not include a measure of the coherence relative to the noise, which would have been necessary to demonstrate SR. The nature of coherence in the ISIH in periodically forced, noisy, physical systems and its relation to physiological data from similarly forced sensory neurons<sup>19</sup> has recently been discussed<sup>26</sup>. Here we use two separate coherence measurements (the  $SNR_{PS}$  and the  $SNR_{ISIH}$ , defined below) to demonstrate SR experimentally in single neurons. These SNRs quantify the information content of the spike train without invoking any specific stimulus-encoding mechanism or neuronal model.

Our experiments used near-field mechanoreceptors, located on the crayfish tailfan, in which small motions of cuticular hairs are transduced by their associated sensory neurons into spikes that propagate centrally along the sensory nerves. In power spectra computed from the spikes (Fig. 1), the main feature due to the periodic signal is the narrow peak at the fundamental frequency riding on a broad noise background. This feature was enhanced by intermediate noise intensities (compare Fig. 1a, and b), but degraded by higher noise intensities (Fig. 1c). Interspike interval histograms (Fig. 2) were obtained at the same three external

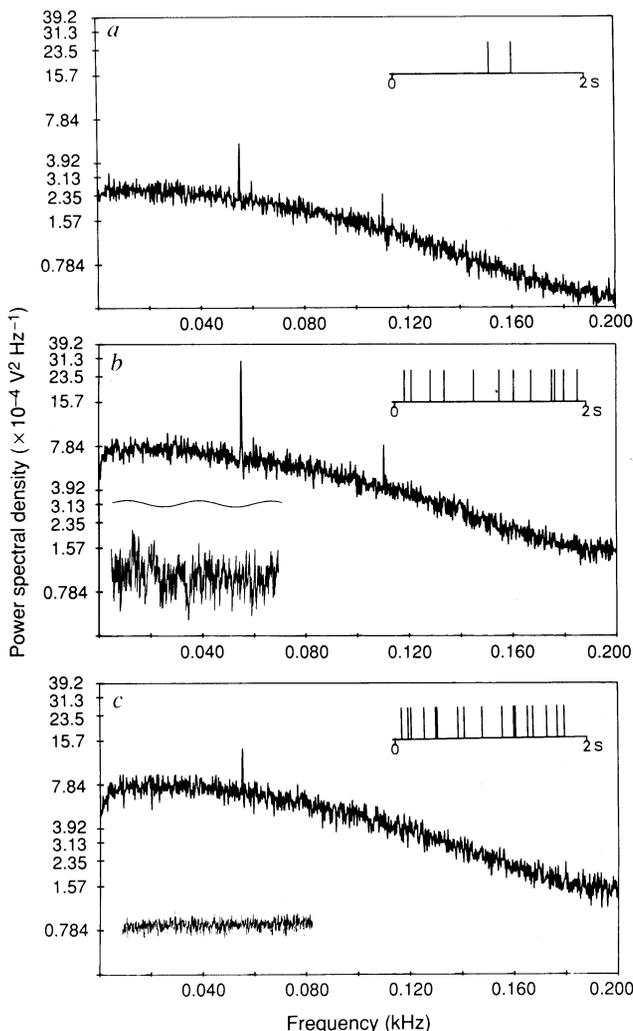


FIG. 1 Power spectra computed from the spiking activity of a crayfish mechanoreceptor, stimulated with a weak signal plus three external noise intensities: a, 0; b, 0.14; c, 0.44 V r.m.s. Insets at upper right show samples of the windowed spike trains from which the power spectra were computed. The total numbers of spikes used for the computations were 698 a, 2,390 b and 4,031 c. All spectra were acquired in the same amount of averaging time, 8.53 min. A single appendage (the telson) was isolated surgically from the crayfish tailfan, together with the associated nerve roots and terminal abdominal ganglion, and immersed in crayfish saline<sup>29</sup> at room temperature. The appendage was mounted vertically on an electromagnetic motion transducer activated by the sum of two inputs: a pure sinusoidal function of 55.2 Hz (the signal), plus a wide-bandwidth gaussian-distributed random function (the noise) as shown in the time series of the signal alone (upper left inset) (b) and the signal plus the noise (lower left inset) (b) and power spectrum (left inset) (c). The sample data shown in the insets were measured for the corresponding conditions stated above for a-c. The noise shown in the insets is quasi-white but the motion transducer introduced a roll-off of about 6.8 dB per frequency decade. The resulting stimulus was thus a combination of periodic and band-limited random motions of the hair relative to the saline, with the intensities of the noise and signal under independent control. Extracellular recordings from a nerve root were windowed to isolate spikes from a single sensory cell. The windowed events were shaped into 3.5-ms rectangular pulses, passed through a low pass (0-1.5 kHz) filter, and digitized at 10 kHz to obtain power spectra and ISIHs. To maximize the effects of the external noise, mechanoreceptors with low spontaneous spiking rates (low internal noise) were chosen for recording. The entire preparation was mounted on a vibration isolation table, the appendage was rotated so as to select the most effective stimulus direction, and a tuning curve was measured to select the most effective signal frequency. The signal intensity was then set slightly above that required for the minimum detectable  $SNR_{PS}$ , and various levels of noise were added to the stimulus. The noise and signal voltages delivered to the electromechanical transducer resulted in a stimulus velocity of  $120 \mu\text{m s}^{-1}$  per V r.m.s. at 10 Hz as determined by an optical calibration. Crayfish mechanoreceptor cells are quite sensitive; without vibration isolation, the cells can easily detect weak building vibrations at 12.5 Hz.

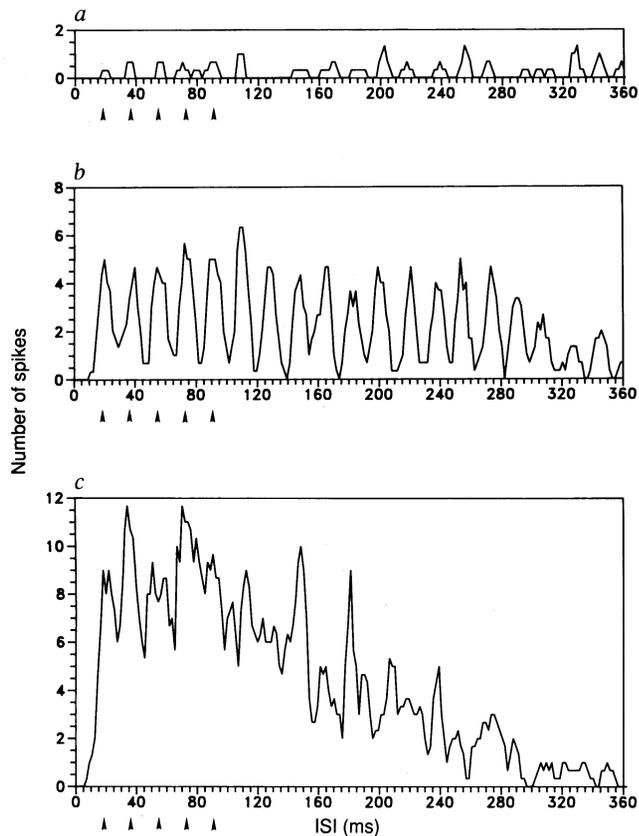


FIG. 2 Interspike interval histograms (ISIHs) obtained under the same conditions used for Fig. 1. To emphasize the coherence of the ISIH peaks with integer multiples of the stimulus period  $T_0$  (18.1 ms), only intervals up to  $20T_0$  are shown. Arrowheads mark the first five integer multiples of  $T_0$ . For clarity these data were smoothed with a three-point moving average. The  $\text{SNR}_{\text{ISIH}}$  calculations (Fig. 3) were obtained from unsmoothed data. The ISIH shown in *b* does not show the more familiar exponential-like decay of peak amplitudes beyond the first peak because the coherent portion of the stimulus is very weak. Under such conditions it is well known<sup>19</sup> that the histogram is spread out over very long time intervals and that the first peak is not the one of maximum amplitude.

noise intensities. With no external noise (Fig. 2*a*) the spike rate was extremely low and most intervals were longer than those shown in Fig. 2. Intermediate noise (Fig. 2*b*) produced a striking growth of coherence marked by an increase in the amplitude of peaks located at integer multiples of  $T_0$ , the stimulus period<sup>26</sup>. Higher noise (Fig. 2*c*) resulted in increasing randomization of the peak structure.

Using various noise intensities, a series of power spectra such as those in Fig. 1 was used to calculate the  $\text{SNR}_{\text{PS}}$  by integrating the data in a small region around the fundamental peak to obtain the strength,  $S$ , the area under the signal peak above the noise. The  $\text{SNR}_{\text{PS}}$ , in decibels, was obtained using the standard definition:  $\text{SNR}_{\text{PS}} = 10 \log_{10} [S/N(f_0)]$ , where  $N(f_0)$  is the amplitude of the broad-band noise background measured at the signal frequency  $f_0$ . The results of these measurements (Fig. 3*a*) show a noise-induced signal enhancement of about 4.5 dB at an optimal noise intensity of  $\sim 0.14$  V r.m.s.

As there is no formal definition of the SNR based on the ISIH, we developed an *ad hoc* definition assuming the occurrences of peaks at integer multiples of  $T_0$  (ref. 26). The interspike intervals located around the first 100 peaks were summed on every interval  $iT_0 \pm T_0/4$  for  $1 \leq i \leq 100$ , and called  $N_{\text{max}}$ . Similarly, the remain-

ing intervals located around the troughs were summed on  $(i-1/2)T_0 \pm T_0/4$  and called  $N_{\text{min}}$ . We then defined the  $\text{SNR}_{\text{ISIH}} = 10 \log_{10} (N_{\text{max}}/N_{\text{min}})^2$ . The results (Fig. 3*b*) parallel those computed from the power spectra: a noise-induced enhancement in the  $\text{SNR}_{\text{ISIH}}$  but with a lower optimal noise intensity of  $\sim 0.10$  V r.m.s.

Not all cells show SR, but we have measured at least some noise-induced enhancement in 10 out of the 11 cells tested. One cell, which had the largest internal noise,  $N(f_0)$ , showed only a monotonic decline instead of a maximum in the SNR.

Our experiment shows very clearly that weak signals can be enhanced by an optimal level of external noise in single sensory neurons. Does this mean that external noise can help crayfish detect weak signals which they could not detect in its absence? Experiments on sensory interneurons and/or behavioural studies will be necessary to answer this question. But a recent psychophysical experiment<sup>27</sup> and model<sup>28</sup> involving human perception of ambiguous figures in the presence of external noise suggest that this is so. □

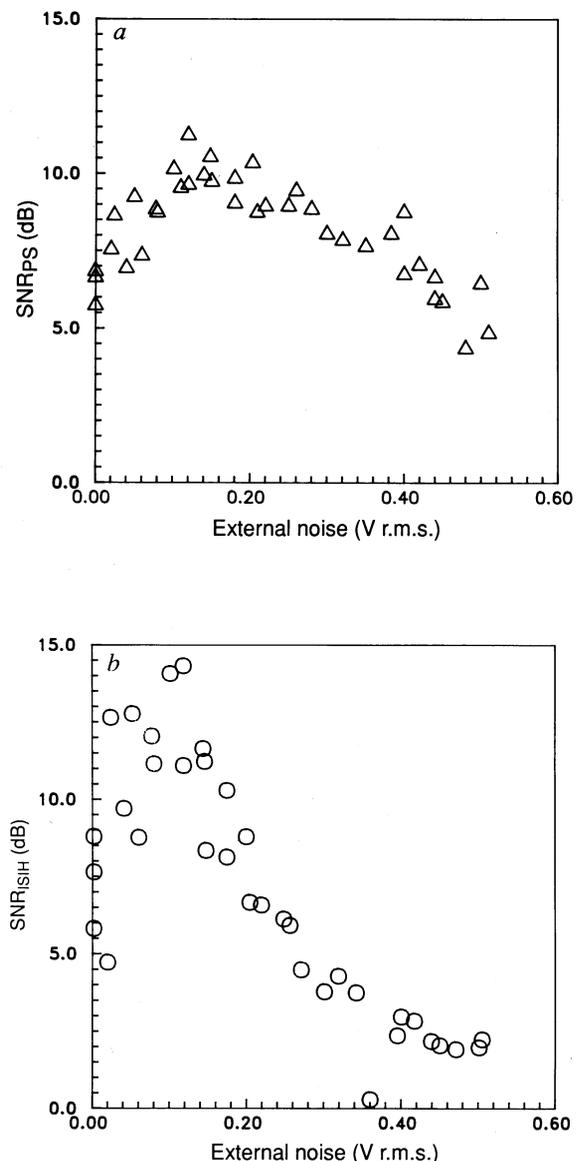


FIG. 3 Stochastic resonance measured from power spectra (*a*) and ISIHs (*b*). The data shown in all figures were acquired from a single representative preparation.

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1. Fauve, S. & Heslot, F. *Phys. Lett.* **97A**, 5–7 (1983).
2. McNamara, B. & Wiesenfeld, K. *Phys. Rev.* **A39**, 4854–4869 (1989).
3. Jung, P. & Hänggi, P. *Europhys. Lett.* **8**, 505–510 (1989).
4. Gammaitoni, L., Marchesoni, F., Meneschella-Saetta, E. & Santucci, S. *Phys. Rev. Lett.* **62**, 349–352 (1989).
5. Moss, F., Bulsara, A. & Shlesinger, M. (eds) *J. stat. Phys.* **70**, 1–514 (1993).
6. Moss, F. in *An Introduction to Some Contemporary Problems in Statistical Physics* (ed. Weiss, G.) (SIAM, Philadelphia, in the press).
7. Benzi, R., Sutera, S. & Vulpiani, A. *J. Phys.* **A14**, L453–L457 (1981).
8. Nicolis, C. *Tellus* **34**, 1–9 (1982).
9. Benzi, R., Parisi, G., Sutera, A. & Vulpiani, A. *Tellus* **34**, 10–16 (1982).
10. Winograd, I. et al. *Science* **258**, 255–260 (1992).
11. Bush, B. M. H. & Laverack, M. S. in *The Biology of Crustacea* Vol. 3 (ed. Bliss, D. E.) 399–468 (Academic, New York, 1982).
12. Mellon, D. J. *exp. Biol.* **40**, 137–148 (1963).
13. Wiese, K. J. *Neurophysiol.* **39**, 816–833 (1976).
14. Moore, G., Perkel, D. & Segundo, J. A. *Rev. Physiol.* **28**, 493–522 (1966).
15. Baño, W. Jr, Fuentes, J. & Segundo, J. *Biol. Cybern.* **31**, 99–110 (1978).
16. Narins, P. & Wagner, I. J. *J. acoust. Soc. Am.* **85**, 1255–1265 (1989).
17. Kaplan, E. & Barlow, R. B. *Jr Nature* **286**, 393–394 (1980).
18. Croner, L., Purpura, L. & Kaplan, E. *Proc. natn. Acad. Sci. U.S.A.* **90**, 8128–8130 (1993).
19. Rose, J., Brugge, J., Anderson, D. & Hind, J. J. *Neurophysiol.* **30**, 769–793 (1967).
20. Knight, B. W. J. *gen. Physiol.* **59**, 734–766 (1972).
21. Gerstein, G. & Mandelbrot, B. *Biophys. J.* **4**, 41–68 (1964).
22. Stein, R. B. *Biophys. J.* **5**, 173–184 (1965).
23. Glass, L., Graves, C., Petrillo, G. & Mackey, M. C. *J. theor. Biol.* **86**, 455–475 (1980).
24. Glass, L. & Mackey, M. C. *J. math. Biol.* **7**, 339–352 (1979).
25. Knight, B. W. J. *gen. Physiol.* **59**, 767–778 (1972).
26. Longtin, A., Bulsara, A. & Moss, F. *Phys. Rev. Lett.* **67**, 656–659 (1991).
27. Chialvo, D. & Apkarian, V. J. *stat. Phys.* **70**, 375–392 (1993).
28. Ditzinger, T. & Haken, H. *Biol. Cybern.* **63**, 453–456 (1990).
29. van Harrevel, A. D. *Proc. Soc. exp. Biol. Med.* **34**, 428–432 (1936).

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